Transferable micromachined piezoresistive force sensor with integrated double-meander-spring system

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Abstract. A developed transferable micro force sensor was evaluated by comparing its response with an industrially manufactured device. In order to pre-identify sensor properties, three-dimensional (3-D) sensor models were simulated with a vertically applied force up to 1000 µN. Then, controllable batch fabrication was performed by alternately utilizing inductively coupled plasma (ICP) reactive ion etching (RIE) and photolithography. The assessments of sensor performance were based on sensor linearity, stiffness and sensitivity. Analysis of the device properties revealed that combination of a modest stiffness value (i.e., (8.19 ± 0.07) N m⁻¹) and high sensitivity (i.e., (15.34 ± 0.14) V N⁻¹) at different probing position can be realized using a meander-spring configuration. Furthermore, lower noise voltage is obtained using a double-layer silicon on insulator (DL-SOI) as basic material to ensure high reliability and an excellent performance of the sensor.

1 Introduction

Rapid development of micro-/nano-fabrication techniques in the past years has had a significant impact not only on higher integration density of the micro-/nano-components leading to enhanced device performance but also on the need of better and more precise quality control of the individual component itself. Consequently, more precise characterizations of physical properties in smaller scale (e.g., micro- or nanoscale) and their know-how are in demand.

As one of the fundamental techniques in material characterization, nano-indentation has already been able to perform measurements at a resolution down to 1 nN with a minimum displacement of < 1 nm. During measurement, this method applies certain loads to create indentation patterns on the sample, which can be used to determine hardness (Fu et al., 2015; Li and Brand, 2013; Nili et al., 2013; Yetna Njock et al., 2016). However, to date there is still no transferable standard available, which can be used for calibrating nano-indentation instruments in the micro- and nano-range. For this purpose, a system for calibrating very small forces is therefore needed. Although different approaches (e.g., piezoelectric: Choi et al., 2016; Lee et al., 2014; Mohan et al., 2015; capacitive: Brand et al., 2016; Viry et al., 2014; Woo et al., 2014; and magnetic flux change: Mehrtash et al., 2015) have been used to realize small force scales. Measuring forces in small scales is also very useful for robotics and medical engineering (e.g., a silicon on insulator (SOI)-based piezoresistive sensor was attached on the tip of the guidewire to detect motions in z axis during the catheterization process) while connecting the micro- and macro-environments is possible by closed-loop disturbance compensation of the system (Mizutani, 2013, 2014; Ousaid et al., 2015).

Micro-fabricated silicon-based force standards for calibrating hardness testing instruments were described in detail elsewhere and are commercially available from Simet-
Figure 1. Three-dimensional (3-D) model of proposed SOI-based micro force sensor (a). Magnified top view of different spring designs (b, c). Cross sectional view of the micro force sensor based on design 1 showing the point loading on the probing area (boss) and the fixing of the sensor to the device holder (d).

Figure 2. Simulated 3-D model of both device configurations (i.e., designs 1 and 2). The color legend shows deflection state on the boss structure in µm (a). The sensor displacement in z direction was computed with a maximum force of 1000 µN (b).

Among them, capacitive, optical, piezoelectric and piezoresistive approaches are most popular. With capacitive sensors, the available measurement range could be limited by the small gap (representing the capacitance) between the probing area of the force sensor and the bottom plate. Measuring small deflections optically is only possible on a reflective surface. Fabrication of an additional reference structure on the probing area and specialized instrumentation are needed to perform reliable deflection measurements. The use of piezoelectric transduction requires deposition of a piezoelectric layer on the spring beam, which may induce residual stress. In contrast, piezoresistive strain gauges can be directly realized using doped silicon resistors; i.e., different robust designs of force sensors are possible by combining standard silicon processing steps.

Recently, a force artifact for the micro-Newton range based on double-sided clamped probing body via combined meander–membrane springs (Doering et al., 2013) were proposed. Meander-type springs in combination with bending springs are well suited to take up the lateral strain, which increases with the deflection of the probing body and are thus able to provide a large linear range of the micro force artifact. Samples of this artifact, which were realized using reactive ion etching (RIE) at cryogenic temperature in silicon, confirm the load-deflection behavior derived from finite element modeling (FEM; Hamdana et al., 2016; Wasisto et al., 2015a). For an application under industrial conditions the micro force artifact comprises a strain-sensing piezoresistive Wheatstone bridge (WB) of very low cross-sensitivity to non-constant ambient conditions such as temperature, humidity and light. Furthermore, noise of the WB limiting the minimally detectable force should be as low as possible. For both low cross-sensitivity and noise, electrical and thermal decouplings of the WB from the membrane spring using a buried SiO₂ layer were proven to be effective (Kähler et al., 2012, 2013). Utilizing this approach, we aim to fulfill the need of small force standards; e.g., for nano-indenters fol-
lowing specifications for small force calibration procedure are required (Table 1).

In this paper, we assess the performance of our fabricated force sensors that have double-meander-spring structures and compare them to industrially manufactured sensor devices. First, mechanical and electrical properties of both designs were numerically analyzed. Afterwards, sensor fabrication was carried out using inductively coupled plasma (ICP) deep reactive ion etching (DRIE) at cryogenic temperature as the key process (Wasisto et al., 2014; Merzsch et al., 2014). Direct-sensing capability of different types of piezoresistive strain gauges (i.e., etched and implanted WBs) was carried out. Furthermore, point-force applications at different positions along the \( x \) axis of the boss structure were carried out to evaluate the sensor performance under conditions corresponding to the typical nano-indenter force calibration procedure.

2 Design and simulation

In this paper, we aim to evaluate the performance of our developed micro force sensor (i.e., design 1) in comparison with the fabricated device from the industry (i.e., design 2). The first step was to model accurate three-dimensional (3-D) representations of both micro force sensors and determine their physical properties (i.e., stiffness and sensitivity) in a finite element simulation using COMSOL Multiphysics 4.3b (COMSOL Multiphysics, 2013). In general, the model geometry was adapted to the actual chip size of the device, i.e., \( 20 \text{ mm} \times 2.2 \text{ mm} \). The sensor geometry consists of a probing area (i.e., boss structure), two meander-beam spring structures and two piezoresistive strain gauge elements (WBs) located at both clamped ends of the device (Fig. 1a). Two designs of the sensor were investigated by employing different spring structure configurations. Design 1 applies deep meander structures perpendicular to the \( x \) – \( y \) plane with small regular gaps between the structures (Fig. 1b), while design 2 adopts a micro-structure with various lateral dimensions and gaps between the structures (Fig. 1c). When a vertical force is applied on the center of the boss structure, a smooth bending of the beams followed by elastic material deformation and changes of resistance values on both WB structures occurred (Fig. 1d). During the simulation, several mesh sizes were used in order to reduce computational time without sacrificing results reliability. In order to replicate the real device conditions, anisotropic single crystal silicon was selected and the 3-D models were rotated by \( 45^\circ \) in the \( x \) – \( y \) plane, allowing for simulations along \(<110>\) crystal orientation (Bonev and Zlatanov, 2002; COMSOL Multiphysics, 2013; Hopcroft et al., 2010).

Numerical simulation of both spring configurations was performed by utilizing several predefined physics interfaces, i.e., solid mechanics and piezoresistivity, domain currents (pzrd). For the mechanical boundary conditions, the bottom part of the SOI-based micro force sensor was given a fixed motion constraint. In contrast, other parts of the models were set to be free. Moreover, the electrical potential boundary condition of 1 V was applied to the input electrode of WB, whereas diagonally opposite output electrode was grounded thereby creating a DC input voltage (\( V_{\text{in}} \)). As a result, changes of the output voltage (\( V_{\text{out}} \)) can be determined through the two remaining WB contacts.

The mechanical and electrical properties of both sensor configurations (design 1 and design 2) were investigated. To capture the behavior of the device in the envisaged application range, vertical forces between 0 and 1000 \( \mu \text{N} \) with a step size of 100 \( \mu \text{N} \) were used. Owing to symmetry considerations, in the following we consider only one of the two meander-beam springs of the sensor. We define the coordinate system origin of the \( x \) axis to be located within the clamped area of the beam. The origin of the \( z \) axis, where the deflection \( z \) direction as a function of an applied force were given, corresponds to a neutral layer of the vertical beam deflection. Along this layer, the longitudinal stress equals to zero. FEM results of different spring configurations under vertical loading up to 1000 \( \mu \text{N} \) are presented in Fig. 2a. Theoretically, the longitudinal stress \( \sigma_L \) in the [110] direction
can be calculated using the following expression (Park et al., 2010):

\[ \sigma_l = \frac{12(l - x)z}{wt^3} F, \]  

(1)

where \( x \) and \( z \) represent the positions on \( x \) and \( z \) axes from the system origin located at the clamping positions and the neutral layer of the membrane springs, respectively. In Eq. (1) the geometrical factors of the beam are given by the beam length \( l \), width \( w \) and thickness \( t \) (Park et al., 2010). Subject to material properties, the stress \( \sigma_l \) can be described as a product of the elastic modulus \( E \) and the longitudinal strain \( \varepsilon_L \) along the \( x \) axis.

\[ \sigma_l = E\varepsilon_L \]  

(2)

At the same deflection state, the mechanical deformation on the WB structures depends on the membrane bending radius \( r \), which can be determined by

\[ r = \frac{z}{\varepsilon_L}. \]  

(3)

Taking geometrical, material and bending properties into account, the force applied on the device can be derived from Eqs. (1)–(3) as

\[ F = \frac{wt^3E}{12r(l - x)^3}. \]  

(4)

The relationship between the applied vertical load \( \Delta F \) and its resulting deflection of the probing body (boss) \( \Delta z \) is referred as device stiffness \( k \):

\[ k = \frac{\Delta F}{\Delta z}. \]  

(5)

Figure 2(b) shows the deflections obtained using FEM with different sensor designs. The vertically applied load on design 1 was incrementally increased and leading to a linear rise of the boss deflection. As a result, design 1 exhibits a stiffness of \((23.39 \pm 9 \times 10^{-3}) \text{ N m}^{-1}\). In comparison, design 2 indicates a stiffer structure response than design 1. In this case, a stiffness of \((100.18 \pm 5 \times 10^{-13}) \text{ N m}^{-1}\) was obtained, which is a factor of \( \sim 4.3 \) higher than that of design 1. A higher stiffness value implicates the requirement of higher applied forces to deflect the structure, which in practical applications can be limited by the instrument or probe to be calibrated. Fine tuning during measurement of very small forces may be problematic since the output signal (i.e., resistance changes of the WB) depends strongly on bending mechanism of the membrane part of the spring. Hence, sensor sensitivity needs to be taken into consideration, which was numerically analyzed by FEM based on the resistance changes \( \Delta R/R \) of the WB (Wasisto et al., 2015b):

\[ \frac{\Delta R}{R} = \sigma_l\Pi_L + \sigma_T\Pi_T. \]  

(6)

where \( \sigma_l, \sigma_T, \Pi_L \) and \( \Pi_T \) are mechanical stresses along longitudinal and transverse directions and piezoresistive coefficients for each direction, respectively. For the WB structures and their electrical contact regions, doping concentrations of \( 5 \times 10^{19} \) and \( 1 \times 10^{19} \text{ cm}^{-3} \) are assumed, respectively. To calculate resistance changes of the WB, a supply voltage \( V_{\text{in}} \) of 1 V was applied diagonally (Wasisto et al., 2015c) and the output voltage \( V_{\text{off}} \) was determined on the opposite diagonal of the resulting full bridge configuration consisting of four resistors (i.e., \( R_1 = R_2 = R_3 = R_4 \)) along \( <110> \) and its transverse direction leads to following relationship between input and output:

\[ V_{\text{off}} = V_{\text{in}} \times \left( \frac{R_2}{R_1 + R_2} + \frac{R_3}{R_3 + R_4} \right). \]  

(7)

Table 1. Required specifications of small force calibration standards for nano-indenters.

<table>
<thead>
<tr>
<th>Force component</th>
<th>Measurement range</th>
<th>Resolution</th>
<th>Resonance frequency</th>
<th>Bandwidth</th>
<th>Chip size</th>
<th>Probing area</th>
</tr>
</thead>
<tbody>
<tr>
<td>( z )</td>
<td>0–1 mN</td>
<td>0.1 µN</td>
<td>&gt;100 Hz</td>
<td>10 Hz</td>
<td>&lt;20 mm x 20 mm</td>
<td>&gt;1 mm x 1 mm</td>
</tr>
</tbody>
</table>

![Image](https://www.j-sens-sens-syst.net/6/121/2017/)
Table 2. Averaged measured sensor calibration values of designs 1 and 2 at different positions on the boss along the longitudinal (x axis, long.) and transverse (y axis, trv.) directions.

<table>
<thead>
<tr>
<th>Sensor design</th>
<th>Stiffness (N m⁻¹)</th>
<th>Force sensitivity (V N⁻¹)</th>
<th>Bending sensitivity (V m⁻¹)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Loading Unloading</td>
<td>Loading Unloading</td>
<td>Loading Unloading</td>
</tr>
<tr>
<td>1 (long.)</td>
<td>8.17 ± 0.08</td>
<td>8.13 ± 0.08</td>
<td>15.35 ± 0.18</td>
</tr>
<tr>
<td>2 (long.)</td>
<td>70.54 ± 2.98</td>
<td>70.59 ± 2.17</td>
<td>4.10 ± 0.64</td>
</tr>
<tr>
<td>1 (trv.)</td>
<td>8.18 ± 0.06</td>
<td>8.23 ± 0.07</td>
<td>15.26 ± 0.32</td>
</tr>
<tr>
<td>2 (trv.)</td>
<td>71.83 ± 1.31</td>
<td>71.49 ± 1.21</td>
<td>4.19 ± 0.49</td>
</tr>
</tbody>
</table>

3 Micro-fabrication

Micro force sensors (design 1) were fabricated using a p-type double-layer silicon on insulator (DL-SOI) wafer with <100> orientation and a resistivity of 0.01–0.02 Ω cm (Active Business Company GmbH, Germany). One major advantage of using DL-SOI wafers is that a defined layer thicknesses can be selected. In this case, we have utilized a DL-SOI wafer with a top layer (device layer), middle layer and bottom layer (handle layer) of (3 ± 1), (25 ± 0.5) and (350 ± 15) μm, respectively. Furthermore, an oxide layer was buried between device and middle layers (BOX1), as well as between middle and handle layers (BOX2). The thicknesses of these layers were (0.2 ± 0.01) μm (BOX1) and (0.5 ± 0.025) μm (BOX2). The use of DL-SOI for design 1 provides better control of the spring and WB structures with respect to the geometrical and doping uniformity. Using this novel approach, the etched WB structures were realized, which are electrically insulated from the underlying spring by the upper buried oxide layer. Thereby, current leakage can be avoided, which occurs by using implanted p-type resistor in n-type bulk silicon as in case of design 2. However, higher...
wafer cost compared to standard bulk silicon material may be set against the use of DL-SOI.

To begin the sensor fabrication, a 4” DL-SOI wafer was cut into 26 mm × 26 mm pieces. Afterwards, the wafer was put into piranha solution (H₂O₂ : H₂SO₄ = 1 : 1) and boiled at 90°C within 5 min to remove organic contamination on the surface (Fig. 4a). This step was performed prior to and after oxidation and before photolithography followed by producing ~ 300 nm thermal oxide on the device layer. Subsequently, a oxide film on a particular contact position was etched and p⁺ diffusion (boron) was performed to obtain a high-quality contact formation (Fig. 4b). In contrast to the WB of design 2, which was prepared by using of implanted piezoresistors, WB structures of design 1 were anisotropically created using ICP DRIE process utilizing O₂ and SF₆ as etch gases at a cryogenic temperature (Sentech Instruments GmbH, Germany; Wasisto et al., 2012, 2013, 2014). In this case, an etching parameter set of an ICP power of 500 W, a high-frequency power of 6 W, an O₂ flux of 7 sccm (sccm is standard cubic centimeter per minute) and an SF₆ flux of 129 sccm at –80°C was utilized (Fig. 4c). Once the WB structures had been fabricated, the oxide layer (BOX1) on the middle of the sensor was removed using a buffered hydrofluoric acid (HF; 6–7%). Following this treatment, a “half-metal” contact (i.e., metal layer was not deposited on the membrane) was realized on the device with 30 nm chromium and 300 nm gold by means of a lift-off process (Figs. 4d, 6). In the next step, photolithography was performed prior to etching of the middle layer. An etching duration of 12–15 min was needed for structuring the middle layer. Thereby, the boss structure was created and the front side of meander structures was defined. The removal of the second oxide layer (BOX2) was carried out by buffered HF (Fig. 4e). The most crucial step during the whole fabrication process was the back-side structuring of the meander spring. A 300 µm deep etching of micro-structures with small gaps (i.e., 50 µm) was performed within ~1.5 h using an ICP power of 500 W, a high-frequency power of 7 W, and a mixture of etch gases of O₂ (6 sccm) and SF₆ (129 sccm) (Fig. 4f).

After completing the fabrication steps, a total of six micro force sensors with chip dimensions of 20 mm × 2 mm were obtained from a 26 mm × 26 mm DL-SOI sample (Fig. 5a). Evaluation in scanning electron microscope (SEM) was performed to analyze the dimensional stability of the realized WB and meander structures. The realized gaps between the meander-spring structures were larger than the designed ones (i.e., around ~60 µm) due to overetching (Fig. 5b). However, this deviation was not crucial to the sensor performance in general (Hamdana et al., 2016). Moreover, this irregularity can be eliminated with fine tuning of the etch recipe, especially regarding the distribution of the process temperature. Furthermore, WB structures show only a small deviation of (7.20 ± 0.10) µm (i.e., below 3%) from each other (Fig. 5c). Hence, a low offset voltage $V_{off}$ (i.e., below 10 mV V⁻¹) was expected, which is very acceptable for the signal processing of the WB.

4 Device characterizations

To determine electrical properties of the sensor, measurements of WB resistances were carried out. The WB resistor arrangement of the sensor (design 1) was shown in Fig. 6. The bridge resistances of both designs were measured under zero applied load to the probing. As shown in Fig. 7, design 1 shows a value of (2979 ± 297) Ω compared to design 2 with a higher resistance but lower standard deviation of (5456 ± 146) Ω. Furthermore, offset voltage values of both devices were also determined. In this case, design 1 has an offset value of (0.05 ± 0.01) mV V⁻¹, whereas design 2 exhibits a higher offset value of (23.15 ± 0.008) mV V⁻¹. The differences of resistor and offset voltage values may be due to material properties and fabrication processes of those two.
types of WB structures. In addition, cross-sensitivities of the fabricated WBs against light, temperature and moisture were determined at a WB supply voltage of 1 V. For measurements under direct illumination with a specific wavelength of 635 nm, a high power cold-light source (KL 1500, Schott AG, Germany) and an optical power meter (Thorlabs GmbH, Germany) were used. Measurements under controlled temperature and moisture were performed in a sealed chamber. Assuming controlled measuring room conditions (i.e., illuminance level < 104 lumen m$^{-2}$, temperature drift < 1 K and relative humidity change < 6 %), we observed changes of offset voltage less than 1 µV corresponding to force errors below 0.1 µN.

During the force application procedure, the sensor was mounted on an aluminum holder of a three axis nanopositioning system. Precise sensor movement with a reproducibility of 5 nm and at resolution of 1 nm was performed against a probing body with a 300 µm ruby sphere, which was mounted on the pan of a compensation balance (Fig. 8a). Thus, the resulting force on the probing area was controlled at a resolution of 1 nN and a reproducibility of 2.5 nN (Peiner and Doering, 2005). Sensor performance was assessed based on calibration on different probing positions on boss structure, i.e., along the x axis (longitudinal) and the y axis (transverse). Total length and increment of 500 and 50 µm were selected during measurements in both longitudinal (long) and transverse (trv) directions, respectively (Fig. 8b–d).

Turning now to the force application procedure, the sensor was fixed on an aluminum holder, which was mounted on a nano-positioning unit. This part can be precisely moved in 3-D directions with a maximum displacement of 100 µm and a resolution of 1 nm. The contact to the sensor was then realized using a stylus with a glued ruby sphere with diameter of 300 µm (Fig. 8a). For both designs, a maximum force of 50 µN was applied and controlled by a compensation balance. Measured values were collected in steps of 400 nm movement along the z axis. In this work, we assessed the sensor responses on force applications at different positions on the probing body (boss). Therefore, the load was applied along the longitudinal axis (i.e., x axis) and the transverse axis (i.e., y axis) through the center of the boss. Between the measurement points (i.e., position 1 and position 2), increment and maximum longitudinal position changes of 50 and 500 µm were used, respectively (Fig. 8b–d).

As shown in Fig. 9a–b, both sensor designs demonstrate good linearity up to 50 µN. Regarding their structural flexibility, design 1 indicates a more compliant behavior with a greater deflection value of boss in the z axis than design 2. Consequently, the first and second derivatives of the force-deflection curve of design 2 exhibit greater values, which indicate the need of higher force to achieve the same deflection. This attribute could be unfavorable for material stability and signal processing. Nevertheless, mechanical properties and sensor stability were investigated by monitoring sen-
Mean device stiffness derived from loading and unloading of different sensor designs are illustrated in Fig. 10a and b. As predicted in the FEM simulations, design 1 exhibits more compliant behavior than design 2. With a mean stiffness value in longitudinal (8.15 ± 0.08) N m⁻¹ and transverse (8.21 ± 0.06) N m⁻¹ directions, the maximum stiffness deviations along the probing area (boss) are below 2% from the mean value (Figs. 10a, 11a). On the other side, design 2 yields a higher mean stiffness (70.57 ± 2.58) (longitudinal) and (71.66 ± 1.26) N m⁻¹ (transverse) with a stiffness deviation up to ~8% from the mean value (Figs. 10b, 11b). This means that design 1 can be deflected with lower force and smaller increments between forces and being less affected by the loading position than design 2. Combining this advantage with sensitivity its high measured mean (15.45 ± 0.17) and (15.34 ± 0.25) V N⁻¹ in longitudinal and transverse directions, respectively and a maximum deviation value of ~3%, the design 1 shows better performance to measure small forces then the design 2 with a maximum deviation in sensitivity of around ~39% (Figs. 10c–d, 11c–d). In terms of bending sensitivity, design 1 yielded mean values in both longitudinal and transverse directions, i.e., (126.59 ± 2.10) and (126.29 ± 2.11) V m⁻¹, with a maximum deviation of ~4%. In contrast, design 2 exhibited bending sensitivity values of (304.47 ± 38.60) and (310.66 ± 33.67) V m⁻¹ with deviations of ~33% (Figs. 10e–f, 11e–f). Tables 2 and 3...
summarize the measurement results on both micro force sensor designs together with the requirements. Therefore, specified parameters of both designs were confirmed experimentally. However, the measurement range is limited between 0 and 50 µN, which has to be extended to 1 mN.

The minimal detectable force of the sensor is limited by the effective noise voltage of the WB. In comparison to a WB with implanted resistances, the SOI-based bridges are electrically isolated to the surrounded substrate by a BOX layer. This allows us to operate it at an AC voltage with no current leakage. For the measurements, we used the MGC plus measuring amplifier system of Hottinger Baldwin Messtechnik (HBM) GmbH with the insert modules ML10B for DC supply and the ML30B for AC supply. The ML30B uses a carrier frequency of 600 Hz. Figure 12a shows the measured noise voltage of the SOI-based micro force sensor (i.e., design 1) with DC and AC supplies. In this case, using an AC carrier frequency, the noise voltage of the micro force sensor in the frequency ranging from 0.1 to 1 kHz could be reduced by a factor of 3. In contrast, the $p$–$n$ junctions of the implanted WBs are massively affected by the potential change between $p$-type WB and the n-doped substrate in case of AC supply to the WB. Figure 12b depicts the noise voltage of an implanted bridge (i.e., design 2) with and without carrier frequency. Applying DC voltage during the measurements, noise voltages varied from 0.1 to 50 Hz have shown more or less the same values. Meanwhile, when the AC voltage was supplied to the bridges, the noise values are > 20 times higher than those at DC supply.

5 Conclusions

This study has set out to measure and assess a developed meander-type sensor for calibration of nano-indenters in the micro-Newton force range compared to an industrially manufactured device. Finite element modeling (FEM) was performed to predict and to provide better understanding of sensor response. The impact on different spring structures (i.e., meander structure for design 1 and combined microstructures of design 2) was investigated through the evaluation of the device properties using FEM and fabricated sensor. Furthermore, repeated measurements by applying vertical loads at different contact points along the $x$ and $y$ axes across the probing body (boss) were performed. While both designs show good measurement linearity, the new one (design 1) has a more flexible structure with higher sensitivity than the industrially manufactured device (design 2). Moreover, design 1 shows an improved behavior concerning the dependence of measured force and deflection on the loading position of the sensor. The loading position can be changed within a range of ±250 µm and force and deflection sensitivity do not change by more than 3%. Furthermore, it has been shown that double-layer silicon on insulator (DL-SOI) material provides better sensor performance in terms of electrical noise. These characteristics will have implications for providing transferable force standards with excellent functionality and high reliability for the micro-Newton scale.
Biographies

Gerry Hamdana received his Bachelor of Engineering degree in mechanical engineering from the Esslingen University of Applied Science in 2012 and Master of Science degree in mechanical engineering specializing in mechatronic/microsystems technology from the Braunschweig University of Technology (TU Braunschweig), Germany, in 2015. Currently, he is pursuing his PhD at the Institute of Semiconductor Technology (IHT), TU Braunschweig, Germany. His research interests include semiconductor processing, microsystems technology and micro-/nano-electromechanical systems (MEMSs/NEMSs).

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Lutz Doering received a Dr.-Ing. degree in micro-electronics technology, precision instrument technology and computer science from the Dresden University of Technology, Dresden, Germany, in 1990. He joined the Department 5.1 Nano- and Micro-metrology, Physikalisch-Technische Bundesanstalt, Braunschweig, Germany, in 2001. His current research interests include characterization and optimization of micromachined cantilever sensors designed for measuring coordinate and roughness parameters and for the transfer of the micro- and nano-Newton force standard to tactile probing tools.

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6 Data availability

Research data are available upon request to the authors.

Competing interests. The authors declare that they have no conflict of interest.

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